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A GPU Implementation of Distance-Driven Computed Tomography

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To the Graduate Council:

I am submitting herewith a thesis written by Ryan D. Wagner entitled "A GPU Implementation of Distance-Driven Computed Tomography." I have examined the final electronic copy of this thesis for form and content and recommend that it be accepted in partial fulfillment of the requirements for the degree of Master of Science, with a major in Computer Science.

Jens Gregor, Major Professor

We have read this thesis and recommend its acceptance:

Gregory D. Peterson, Stanimire Tomov

Accepted for the Council:

Dixie L. Thompson

Vice Provost and Dean of the Graduate School

(Original signatures are on file with official student records.)

A GPU Implementation of Distance-Driven Computed Tomography

A Thesis Presented for the

Master of Science

Degree

The University of Tennessee, Knoxville

Ryan D. Wagner

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Abstract

Computed tomography (CT) is used to produce cross-sectional images of an object via noninvasive X-ray scanning of the object. These images have a wide range of uses including threat detection in checked baggage at airports. The projection data collected by the CT scanner must be reconstructed before the image may be viewed. In comparison to filtered backprojection methods of reconstruction, iterative reconstruction algorithms have been shown to increase overall image quality by incorporating a more complete model of the underlying physics. Unfortunately, iterative algorithms are generally too slow to meet the high throughput demands of this application. It is therefore worthwhile to investigate methods of improving their execution time. This paper discusses multiple implementations of iterative tomographic reconstruction using the simultaneous iterative reconstruction technique (SIRT) and the distance-driven system model. The primary focus is an implementation of the branchless variant of the distance-driven system model on a graphics processing unit (GPU). Solutions to key implementation concerns which have been neglected in previous literature are discussed.

Table of Contents

1	Introduction	1
1.1	The Purposes and Uses of Computed Tomography	1
1.2	Projection Data	2
1.3	Scanner Geometry	3
1.4	Reconstruction Methods	5
1.5	System Models	6
1.6	GPU Implementation	6
2	Iterative Reconstruction	8
2.1	The Simultaneous Iterative Reconstruction Technique	8
2.2	SIRT Applied to Statistically Weighted Least Squares	10
2.3	Image Convergence	10
3	System Models	13
3.1	General System Models	13
3.2	Distance-Driven System Model	14
3.2.1	Distance-Driven in Two-Dimensions	15
3.2.2	Distance-Driven in Three-Dimensions	17
3.2.3	Distance-Driven Branchless Modification	18
4	Implementation	22
4.1	Naive Branched Implementations	22

4.2	Branched Implementation	23
4.3	Branchless Implementations	25
4.3.1	Computation of Integral Image and Integral Rays	26
5	Results and Discussion	30
5.1	Performance Comparison	30
5.2	Potential Performance Improvements	33
5.3	Image Quality	34
5.3.1	Floating-Point Precision	34
5.3.2	Texture Interpolation	34
5.3.3	Border Elements	35
5.3.4	Ray Value Leakage	37
5.3.5	Reconstructed Images	38
6	Conclusion	41
	Bibliography	43
	Vita	47

List of Figures

1.1	A selection of source and detector arrangements.	3
1.2	The coordinate system and geometry.	4
2.1	The average weighted projection data error of an image quality bag reconstruction over 23 iterations.	11
2.2	Reconstructed image quality bag after various iterations	12
3.1	Illustration of the line intersection model	14
3.2	Illustration of a voxel-driven method	15
3.3	Voxel and detector mappings at different rotation angles	16
3.4	Rectangular sum computation	18
3.5	Integral image summation where all voxel values and areas are 1	19
3.6	Computation of an image plane's contribution to a ray value	19
3.7	Mapping of detector array to common plane	21
4.1	Code excerpt for computation of weighted row overlap	24
4.2	Code excerpt for computation of weighted column overlap	25
4.3	Interpolation from mapped detector elements to a uniform grid	28
5.1	Comparison of single iteration reconstruction time	31
5.2	Speedup of single iteration reconstruction time	32
5.3	Comparison of row sum values produced with various voxel size to detector size ratios	35
5.4	Forward projection output with and without border voxels	36

5.5	Illustration of ray value leakage in the integral rays	38
5.6	The effects of ray value leakage	38
5.7	Artifacts resulting from ray value leakage	39
5.8	Reconstruction of image quality bag	40
5.9	Reconstruction of resolution bag	40

Chapter 1

Introduction

1.1 The Purposes and Uses of Computed Tomography

Computed tomography (CT) is primarily used in situations where tomographic, or cross-sectional, views of an object are required and it is not possible to cut into the object physically. CT scans are typically employed in medical settings to aid in diagnostic medicine. Another application – most relevant to this thesis – is the detection of security threats in checked airport luggage. CT scans allow for automated or manual examination of luggage contents for hazardous materials or other potentially dangerous items and are part of the last line of defense for preventing these threats from being loaded onto an aircraft [1]. CT scanners are well suited for this task due to their ability to create tomographic images, which can be used to estimate density and volume of objects in the luggage. If the density and volume of an object is suspect, it can be automatically flagged for further inspection [2].

1.2 Projection Data

The data used to create tomographic images is generated by passing X-rays through the object of interest and detecting the rays on the other side of the object. As the rays pass through the object, they are attenuated, or reduced in intensity, primarily through the processes of photoabsorption and compton scattering. Different materials have different coefficients of attenuation, and the longer an X-ray travels through a material, the more it will be attenuated. Measuring the intensity of a ray which has passed through an object and comparing it to the original intensity allows for the computation of the attenuation and aids in determining its material makeup [3]. Multiple X-ray images, referred to in this paper as projections or views, are taken of the object at different angles to generate the projection data. This projection data is then processed to produce tomographic images.

By approximating the X-ray transmitted intensity as a monoenergetic beam, the Beer-Lambert Law (1.1) can be used to determine the intensity I_1 of radiation with initial intensity I_0 as it travels through an object with a spatially variant attenuation coefficient μ dependent on coordinates x , y , and z along line, or ray, L :

$$I_1 = I_0 e^{-\int_L \mu(x,y,z) dl} \quad (1.1)$$

which can also be expressed as:

$$\int_L \mu(x, y, z) dl = -\log \frac{I_1}{I_0} \quad (1.2)$$

By discretizing the object as an image grid of elements with individual attenuation values, and with a discrete number of views and rays, this can be represented as a linear system $Ax = y$, where

$$A \equiv \int_L dl \quad x \equiv \mu(x, y, z) \quad y \equiv -\log \frac{I_1}{I_0} \quad (1.3)$$

Note the projection data y is the negative log of the measured intensity divided by the initial intensity. In practice, a blank scan with no object in the gantry is used to represent the initial intensity. Later, this blank scan is used to log normalize the projection data before reconstruction.

1.3 Scanner Geometry

System geometry describes the physical attributes and parameters of the CT scanner used to generate the projection data. Early scanners used a parallel beam geometry in which a single source and detector shift up and down before rotating to collect data from multiple parallel beams; fan beam geometries use a single source and a column of detectors; and cone beam geometries collect data in two-dimensions using a single source and a 2D array of detectors. Detector arrays are generally either flat or curved panel arrays. Flat panel detector arrays have equidistant columns of detectors and curved panel detector arrays have equiangular detector columns. 2D images are generated by scanners with a single column of detectors, and 3D images are typically generated by scanners with a 2D array of detectors [4]. Figure 1.1 shows examples of parallel, fan, and cone beam geometries.

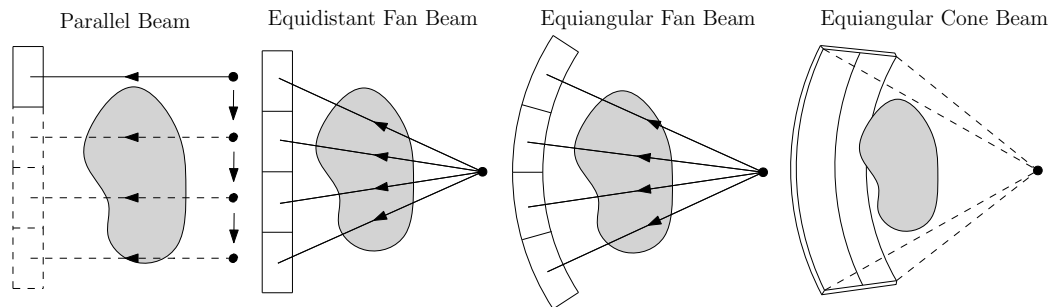


Figure 1.1: A selection of source and detector arrangements.

When a 3D object is longer than the width of the detector array, a helical scan is performed by adding a pitch to the detector and source rotation. The development of helical scanners was motivated by the desire to scan an entire human organ in

a single breath. Cone beam helical scanners were later developed to improve the isotropic spatial resolution [5]. Figure 1.2 shows the coordinate system and geometry used in this research. Note the luggage being scanned moves down the gantry in the positive z direction.

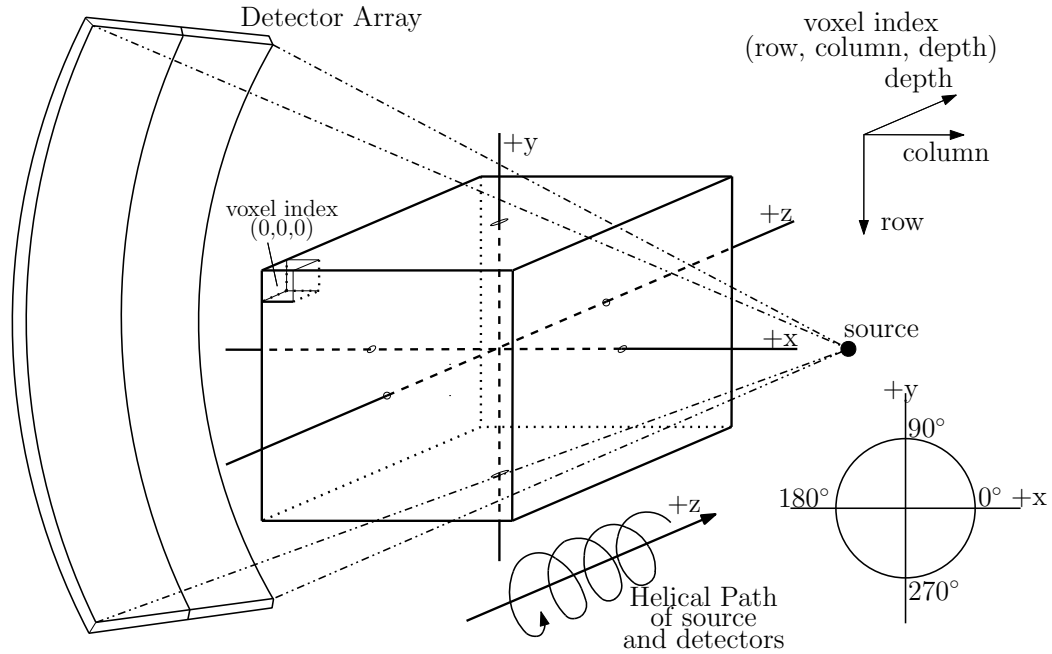


Figure 1.2: The coordinate system and geometry.

The system geometry used in this research is as follows:

- Helical, cone beam scanner
- 120mm pitch
- Equiangular detector array of 720 detector rows and 56 detector columns
- 2mm x 2mm detector pixels
- 1000 projections per rotation with 5 rotations
- 1500mm source to detector distance
- 900mm source to isocenter distance
- Translation in the z direction

The projection data used for reconstruction was provided via simulation by Morpho Detection LLC and consists of two separate data sets. The first is a bag used

to test image quality. Notable contents include a water cylinder, scatter phantom (delrin block), aluminum bar, teflon bar, and a string of metal spheres. The second bag is designed to test resolution and penetration. It includes a block with resolution bars and a second with thin wires. It also contains a highly attenuating lead block.

1.4 Reconstruction Methods

Image reconstruction techniques are generally divided into analytic and iterative methods. The analytic methods, such as filtered back-projection, approximate the solution using a closed form equation [5]. The iterative methods take either an algebraic approach to solve for the solution to the linear system as described in §1.2, or a statistical approach which maximizes a likelihood of the measurements [6]. The analytic methods are the most commonly used in commercial settings, primarily because closed form solutions are more computationally efficient than iterative methods [2, 5]. Despite the difference in overall reconstruction time, iterative reconstruction methods are preferable in some situations because of their potential to improve image quality by incorporating a more complete model of the underlying physics. Iterative methods are able to produce better images when working with incomplete data, such as limited view angles or opaque objects in the field of view [7, 8]. Thibault et al. showed that iterative methods can also be used to provide more accurate noise and complex geometry modeling as well as higher image resolution and reduced helical artifacts [9]. Due to these image quality advantages of iterative methods, it is desirable to investigate ways of increasing their reconstruction speed. Chapter 2 describes the simultaneous iterative reconstruction technique which is the reconstruction method used in this research. Other reconstruction algorithms could be easily substituted, and the algorithm itself is not the focus of this work.

1.5 System Models

The system matrix A used in iterative reconstruction methods is determined by the system model. There are many methods for defining this matrix and most can be considered to be either ray or voxel-driven methods. Ray-driven methods follow the path of a ray through the image space and assign values to the elements in the ray's row based on its interaction with individual voxels. On the other hand, voxel-driven methods project an individual voxel onto the detector array for each view to determine the voxel's interaction with each ray to compute a column of the system matrix. The distance-driven system model is a third method for computing this system matrix. This method allows for the computation of rows or columns of the system matrix at a time. The edges of rays and voxels are mapped to a common plane to determine the overlap between them. This overlap is combined with the length of intersection between the ray and the slab of voxels parallel to the common plane to determine system matrix values. This paper focuses on iterative image reconstruction using the distance-driven system model. Chapter 3 expands on ray and voxel-driven models and describes the various forms of the distance-driven system model.

1.6 GPU Implementation

The image quality advantages of iterative reconstruction methods would imply wide adoption. However, their slow reconstruction time is a major limiting factor. For example, the ability to produce higher quality and more accurate reconstructions would decrease the difficulty of identifying threats in checked bags. Despite this, the high reconstruction time is prohibitive because the scanning systems must be able to quickly produce results to manage the high volume of bags processed in airports. One common method of improving algorithm runtime is by exploiting parallelism. Existing literature has succeeded in improving the reconstruction time of this method using the high level of parallelism provided by GPUs [10, 11]. However, this task

is not straightforward, and these papers provide few implementation details. This research outlines some of the difficulties of implementation, provides a solution, and discusses how future improvements could be made. Chapter 4 provides details on the implementation of distance-driven image reconstruction, and Chapter 5 discusses results and performance.

Cuda is an application programming interface created by NVIDIA for the programming of NVIDIA GPUs using C [12]. Other languages such as C++ and Fortran are also supported. When programming a GPU using Cuda, both the CPU and GPU are used. The host refers to the CPU and main memory, while the device refers to the GPU and its onboard memory. The host is capable of copying and moving memory to and from the device and within the device itself. It is also able to call functions known as kernels which execute on the device. In this way, it is possible to interleave CPU and GPU computation. However, in the implementations discussed here, the majority of the work is performed on the GPU after the host copies all relevant data to the device.

The individual unit of execution in Cuda is a thread. Threads are grouped into blocks and blocks are grouped into grids. Warps are groups of 32 threads within a block that are created and executed together. Threads in a warp execute the same instruction at the same time. However, if these threads reach a data-dependent conditional branch, the two paths of the branch must be executed serially with the threads not on the current path disabled.

In general, threads on a GPU execute more slowly than threads on a CPU. However, significantly more threads can be executed at a time on a GPU than on a CPU. Therefore, given a sufficiently parallel workload, a GPU will provide better throughput.

Chapter 2

Iterative Reconstruction

As mentioned in §1.2, the relationship between the image and projection data can be represented as a linear system. Because it is typical for there to be significantly more rays than voxels, this system is expected to be overdetermined [4]. The result is that this linear system cannot be solved directly [3]. Therefore, the goal is to compute an approximation, x , of the scanned object.

2.1 The Simultaneous Iterative Reconstruction Technique

The simultaneous iterative reconstruction technique (SIRT) is one choice for solving this linear system [4]:

$$x^{(k+1)} = x^{(k)} + \alpha CA^T R(y - Ax^{(k)}) \quad (2.1)$$

The variable k represents the iteration. The initial image $x^{(0)}$ can take any value. The closer it is to an accurate representation the object, the faster the iteration will converge. It is possible to compute a less accurate approximation of the object to use as $x^{(0)}$, such as by filtered backprojection; however, in this research all elements are

initialized to zero. The matrix $C = \text{diag}\{1/c_i\}$ is a diagonal preconditioning matrix whose elements are inverse column sums c_i of the system matrix A . Similarly, the matrix $R = \text{diag}\{1/r_i\}$ is a diagonal matrix of inverse row sums r_i . The vector y is the log normalized projection data. The relaxation parameter α defines the step size, and was shown to have an optimal value of $2/(1 + \epsilon) \approx 1.99$ [13]. The operation $Ax^{(k)}$ is the forward projection. It computes ray values based on the current image approximation. The resulting ray values are then subtracted from the projection data and weighted by the system matrix row sums to determine the error between the observed and approximated projection data. The backprojection operation multiplies the transpose of the system matrix and this projection data error and weights it by the column sums to produce an update to the image approximation.

Let the weighted projection data error be e . Then, in 3D forward projection, the weighted projection data error for a ray i is computed as:

$$e_i^{(k)} = \frac{1}{r_i} (y_i - \sum_{j \in I} a_{ij} x_j^{(k)}) \quad (2.2)$$

where I is the set of all voxels. Let the u be the image update vector. Then the update value for voxel j is computed as:

$$u_j^{(k)} = \frac{1}{c_j} \sum_{i \in D} a_{ij} e_i^{(k)} \quad (2.3)$$

where D is the set of all rays. Equation 2.1 can be rewritten as:

$$x^{(k+1)} = x^{(k)} + \alpha u^{(k)} \quad (2.4)$$

2.2 SIRT Applied to Statistically Weighted Least Squares

Though SIRT is an effective method of producing a reconstructed image, it can be improved by the addition of statistical weighting. Sauer and Bouman showed that a statistical model of the projections as Poisson-distributed random variables leads to a weighted least squares problem $x^* = \operatorname{argmin}(F(x))$, where $F(x) = \frac{1}{2} \|y - Ax\|_W^2$ [14]. The weight matrix W is a diagonal matrix of the variance associated with each ray. Therefore, $W = \operatorname{diag}\{\lambda_i e^{-y_i}\}$ where λ_i is the initial intensity of ray i . This weighted least squares problem can be solved using preconditioned gradient descent as $x^{(k+1)} = x^{(k)} - \alpha D \nabla F(x^{(k)})$, where D is a preconditioning matrix. In comparison, SIRT solves a geometrically weighted least squares problem $x^* = \operatorname{argmin}(\frac{1}{2} \|y - Ax\|_R^2)$ [6]. This R weighting is based on the amount of intersection between each ray and the image and therefore, the more a ray intersects the image, the larger its error tolerance [6]. In the case of noisy data, a statistical weighting is preferable. Gregor and Fessler showed that SIRT can be modified to include this statistical weighting via a variable transformation to solve the weighted least squares problem using preconditioned gradient descent [6]. A is modified to be $\tilde{A} = [\tilde{a}_{ij}]$ where $\tilde{a}_{ij} = w_i r_i a_{ij}$, and therefore, \tilde{C} is a diagonal matrix of inverse column sums of \tilde{A} and \tilde{R} is a diagonal matrix of inverse row sums of \tilde{A} . The projection data y is modified to be $\tilde{y} = w_i r_i y_i$. Then, this modified SIRT is given as $x^{(k+1)} = x^{(k)} - \alpha \tilde{C} \nabla F(x^{(k)}) = x^{(k)} + \alpha \tilde{C} \tilde{A}^T \tilde{R} (\tilde{y} - \tilde{A} x^{(k)})$ and can be simplified to $x^{(k+1)} = x^{(k)} + \alpha \tilde{C} A^T W (y - Ax^{(k)})$.

2.3 Image Convergence

As the reconstruction algorithm iteratively improves the image approximation, the average weighted projection data error decreases. This average error serves as a good metric for the rate of convergence. Figure 2.1 shows this average error over 23 iterations of the image quality bag. Note the error decreases quickly for the

first few iterations as the major bag features start to form and slows down as the details are improved. Given a sufficient number of iterations, the average error will converge to a fixed value; however, complete convergence is not typically required and reconstruction is terminated after a fixed number of iterations or once the average error passes a threshold. Figure 2.2. shows the improvement of image quality for a selection of iterations.

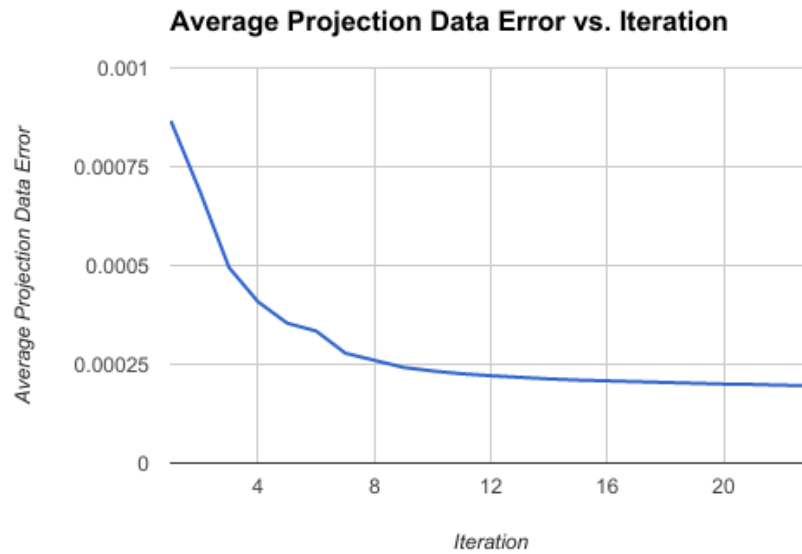


Figure 2.1: The average weighted projection data error of an image quality bag reconstruction over 23 iterations.

The rate of convergence can be increased through a method known as ordered subsets [15]. Nearby rays are likely to contain similar or redundant information; therefore, orthogonal rays are expected to provide the most new information. The projection data is then divided into subsets which prioritize the distance between rays in a subset and rays in subsequent subsets. An iteration of the reconstruction algorithm is then divided into subiterations which update the image using only the rays in the subset. Use of ordered subsets was not pursued in this work.

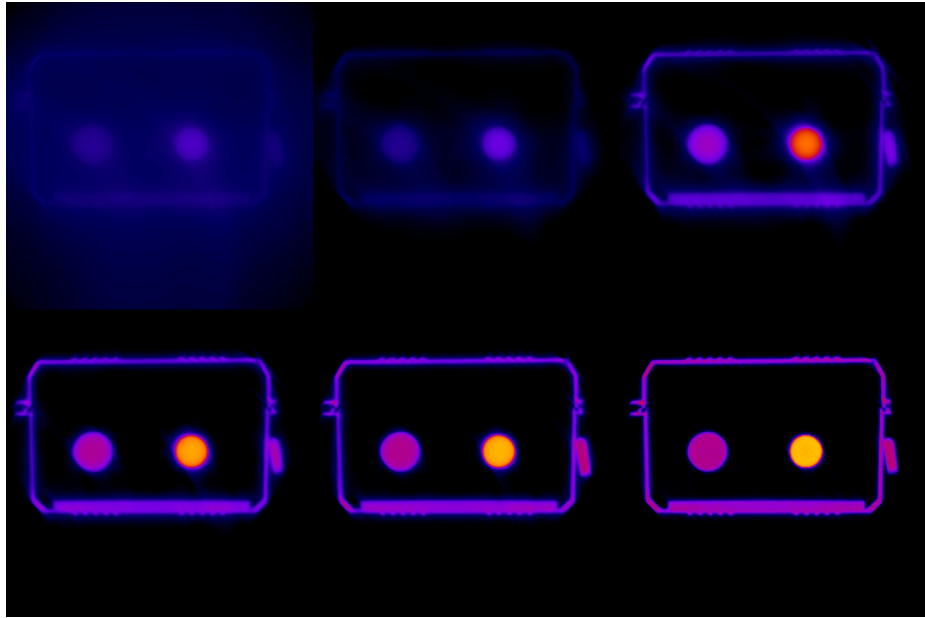


Figure 2.2: A slice through the image quality bag showing cross section of the teflon bar (left) and water bottle (right). Iterations shown are: 1, 2, 10, 20, 30, 57. Image lookup table used is fire. Colors in order of increasing value are: blue, red, yellow, white.

Chapter 3

System Models

3.1 General System Models

Each row of the system matrix represents a projection ray and each column represents an image voxel. Therefore, each element in A is a quantification of the voxel's potential to attenuate the ray. There are many system models, or methods for creating this system matrix, and they are integral to the iterative reconstruction process. The quality of the reconstructed image is dependent on the accuracy of the system matrix [3]. Since the size of the system matrix is the number of projection data values multiplied by the number of image voxels, it is typically too large to store in memory. Instead, elements of the system matrix are computed as needed. This computation accounts for a significant percentage of the overall reconstruction time; therefore, the generation of the system matrix must balance accuracy and computational cost [3].

System models can typically be divided into two classes: ray or voxel-driven methods. Ray-driven methods follow the path of a ray through the image and calculate a row of the system matrix at a time. Voxel – or pixel in the 2D case – driven methods iterate through the voxels and calculate a column of the system matrix at a time [3]. An example of a ray-driven approach is the line intersection model (Fig. 3.1). Rays are represented as a line drawn from the source to the center of a detector. The

value of an element $a_{i,j}$ in the system matrix corresponds to the length of intersection between the ray i and the voxel j [3]. There are computationally efficient methods for computing this model such as Siddon's method [16] and an improved version by Jacobs [17]. Unfortunately, the line intersection approach suffers from ring artifacts for cone beam data due to the approximation of the volumetric x-ray beam as a line [18]. A method which almost completely eliminates these ring artifacts at the cost of additional computation, uses interpolation to assign support values: Interpolation coefficients are determined for the nearest voxel centers at equally spaced points on the ray. These coefficients then determine the support provided by the ray to those nearest voxels [3]. An example of a simple voxel-driven approach computes system matrix elements as follows (Fig. 3.2): for each projection, compute the coordinates of each detector center; compute the line from the source through a voxel to the detector plane and find the intersection point with the detector plane; use interpolation between the intersection point and the values of the bounding detectors to compute their approximate contribution [19].

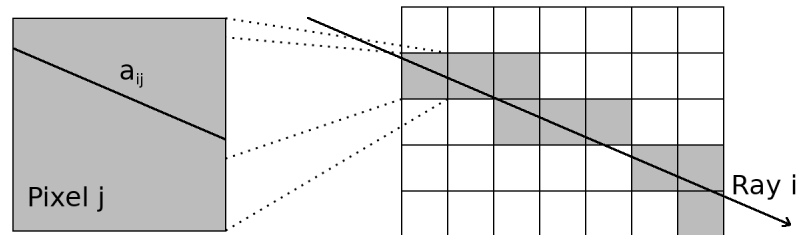


Figure 3.1: Illustration of the line intersection model

3.2 Distance-Driven System Model

A system model which does not fit into ray or voxel-driven categories is the distance-driven model, developed by De Man and Basu in 2003 [20]. The distance-driven system model has similarities to both ray and voxel-driven methods and can compute either system matrix rows or columns. This is in contrast to the ray-driven methods which only compute system matrix rows and the voxel-driven methods which only

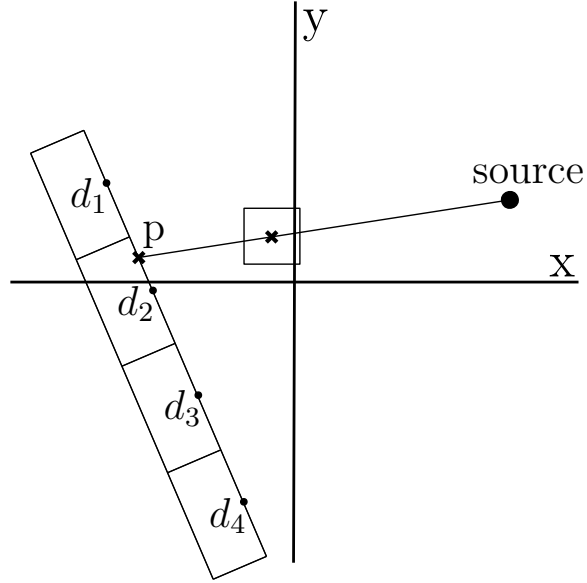


Figure 3.2: Illustration of a voxel-driven method

compute system matrix columns. This simplifies the parallelization of the distance-driven method. It is possible to directly compute entire ray values during projection and entire voxel values during backprojection instead of having to compute partial values during ray-driven backprojection and voxel-driven forward projection.

3.2.1 Distance-Driven in Two-Dimensions

During forward and back projection in 2D, both the detectors and the pixels are mapped to a common axis. The choice of common axis depends on how the rotation of the scanner is represented in implementation. The mapping is done by determining the line between the source and the point to be mapped then finding its intercept with the common axis, as shown in Figure 3.3.

In a traditional case, the pixels are fixed relative to the coordinate system and the source and detectors are rotated around the image. As a result, whichever axis is most orthogonal to the current source rotation angle is chosen. When mapping to the x axis, the pixel edges to the left and right are mapped, while when mapping the y axis

the top and bottom pixel edges are chosen (Fig. 3.3). This results in non-overlapping pixel mapping within image slabs parallel to the common axis.

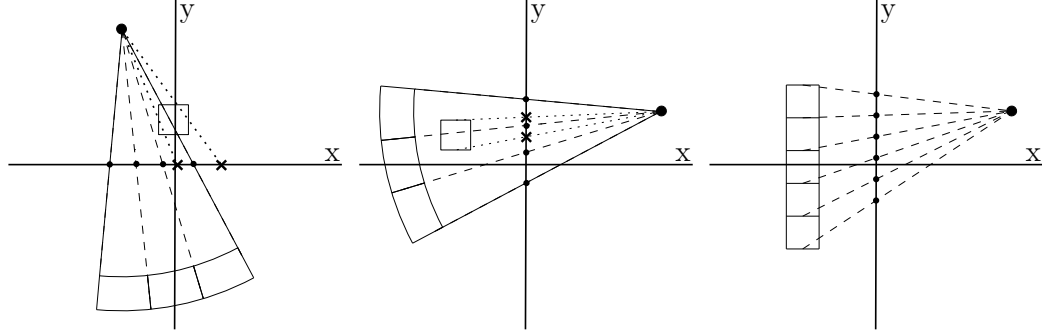


Figure 3.3: Pixel and detector mappings at different rotation angles. Left maps the center of the left and right pixel edges to the x axis. Center maps the center of the top and bottom pixel edges to the y axis. Right shows that pixel mappings of image slabs are uniform and non-overlapping.

The system matrix value for ray i and pixel j is:

$$a_{ij} = \frac{t}{\cos \phi} \frac{o_{ij}}{w_i} \quad (3.1)$$

where t represents the width of the pixel in the dimension orthogonal to the common axis, ϕ represents the angle between the ray and the axis orthogonal to the common axis, o_{ij} represents the amount of overlap between the mapped pixel and detector, and w_i represents the width of the mapped detector. The component $\frac{t}{\cos \phi}$ is known as the slab intersection length. It is a measurement of the distance a ray travels through a slab of pixels. In 2D, a slab of pixels is an image row when mapping to the x axis and an image column when mapping to the y axis. The component $\frac{o_{ij}}{w_i}$ represents the fraction pixel j overlaps ray i . This calculation can be thought of intuitively as follows: Each ray travels through an image slab for a distance given by the slab intersection length. Because pixels in an image slab are non-overlapping and are parallel to the common axis, they also map to the common axis in a non-overlapping way. Therefore, each pixel in an image slab is assigned a fractional part of the slab intersection length based on how much it overlaps with the ray.

It is also possible to fix the source and detectors and rotate the image pixels instead. In this case, the common axis is chosen based on preference and does not change. As the voxels rotate, the edges chosen to be mapped will be the edges most parallel to the common axis. Representing rotation through the image can simplify implementation, but it has the disadvantage that voxel mappings within image slabs are no longer non-overlapping.

3.2.2 Distance-Driven in Three-Dimensions

In 2004, De Man and Basu described distance-driven projection and backprojection in 3D [21]. The extension of the distance-driven method is straightforward. With the addition of the z dimension, we now map to a common plane instead of a common axis. This plane will be either the x - z plane or the y - z plane depending on the current angle of rotation. Image slabs in 2D are rows or columns of pixels, while in 3D they are planes of voxels and are parallel to the common plane. Therefore, the calculation for the slab intersection length $\frac{t}{\cos \phi \cos \gamma}$ now includes division by $\cos \gamma$ where γ is the angle of the ray in the z direction from the axis orthogonal to the common plane. Note that ϕ is determined by the rotation of the detectors and the row of the detector, and γ is dependent only on the detector column. The mapping of voxels and detectors now includes a second dimension. Voxels and detectors will overlap in both the x or y dimension and the z dimension. The computation for an element of the system matrix is now the length of the ray through the voxel's slab multiplied by the ratio of the area of voxel-detector overlap and the area of the detector:

$$a_{ij} = \frac{t}{\cos \phi \cos \gamma} \frac{o_1}{w_1} \frac{o_2}{w_2} \quad (3.2)$$

Where o_1 and w_1 are the overlap and ray width in the x or y dimension depending on which axis is being mapped to, and o_2 and w_2 are the overlap and ray width in the z dimension.

3.2.3 Distance-Driven Branchless Modification

In 2006, De Man and Basu introduced the branchless distance-driven method developed with the intent of improving performance in deeply pipelined and single instruction multiple data architectures by eliminating the conditional inside the inner overlap kernel that determines whether the next edge is associated with a voxel or a ray [22]. Instead of checking the overlap of each voxel and detector individually, some initial computation is performed to find the overlap between a ray and an entire image plane or a voxel and all the rays of a projection in a single step. Consider a ray and image slab mapped to the common plane. For forward projection, the contribution of this slab of voxels to the ray value is the integral of the mapped image slab with bounds of the ray borders. When the mapped ray and voxel borders are in line with each other, the integral can be represented as the sum of the voxels multiplied by their respective areas. Further, note any such rectangular sum can be computed from the sums for each of the four rectangles created by the origin corner of the image slab and the four corners of the rectangle (Fig. 3.4). The values of all such rectangles in a plane can be computed simply.

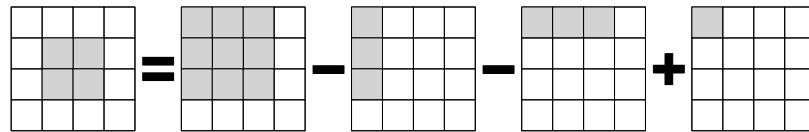


Figure 3.4: Rectangular sum computation

The conditional in the inner loop of the distance-driven kernel is eliminated by pre-integrating the voxel values. Pre-integration is performed for forward projection in the following way: The image is divided into planes, called image slabs, parallel to the common plane. Each of these image slabs is then integrated in two dimensions, producing an integral image. The integral image planes are formed by summing voxel values along rows and then columns such that the value of a voxel in the integral image is the sum of its own value and the values of all the voxels behind and above it in its

plane (Fig. 3.5). To properly represent the integral, each voxel value is also multiplied by the mapped voxel area.

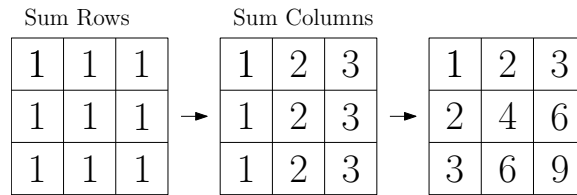


Figure 3.5: Integral image summation where all voxel values and areas are 1

Once the integral image is created, the ray values can be computed by mapping individual rays to the plane, accessing the integral image values at the corners of the mapped ray, and computing the plane’s contribution to the ray value according to Figure 3.6. When ray corners do not line up with voxel boundaries, bilinear interpolation is used to approximate the integral image values.

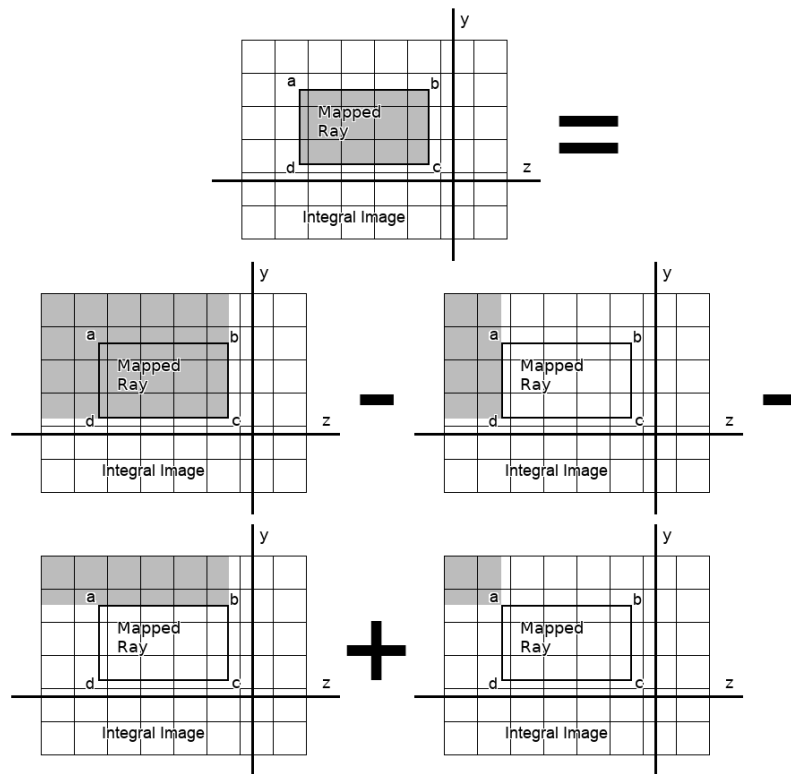


Figure 3.6: Computation of an image plane’s contribution to a ray value

Therefore, (2.2) can be rewritten as:

$$e_i = \frac{1}{r_i} \left(y_i - \frac{t}{\cos \phi \cos \gamma} \frac{\sum_{j \in S} c_j - d_j - b_j + a_j}{w_1 w_2} \right) \quad (3.3)$$

where S is the set of image slabs for the current projection, and c_j , d_j , b_j , and a_j are the values from integral image j accessed at the corners of the mapped ray i as shown in Figure 3.6.

This process becomes more complicated during backprojection. Instead of voxel values, ray values for each view are summed to produce integral ray values. Because the slab intersection length is dependent on the ray, this value is included. As with the creation of the integral voxels, each element should be multiplied by its mapped area; however, since the calculation of system matrix values includes a division by the area of the mapped detector, this cancels out and does not need to be included. Unlike mapped voxels, mapped rays are not completely uniform. As rays deviate from orthogonality with the common plane, their mappings increase in size. However, because the detector array is not curved along rows, rays map uniformly in height and width on a per row per projection basis. Figure 3.7 shows a projection mapped onto a coordinate grid at orthogonal and 45° angles. The non-uniform ray widths and heights between rows prevents simple summation of the ray values as is possible with voxel values. A solution to this issue is discussed in §4.3. Once the integral rays have been computed, they are accessed in the same way as the integral voxels. Therefore, Figure 3.6 applies when the integral image is replaced with the integral rays and the mapped ray is replaced with a mapped voxel. Equation 2.3 can be rewritten as:

$$u_j = \frac{1}{c_j} \sum_{i \in V} c_i - d_i - b_i + a_i \quad (3.4)$$

where V is the set of projection views, and c_i , d_i , b_i , and a_i are the values from the integral rays for view i accessed at the corners of the mapped voxel j . The slab intersection length and division by w_1 and w_2 are included in the values from the

integral rays as they are dependent of the ray. Since the computation of the integral rays must include a multiplication by the ray's mapped area to properly represent the integral as a summation, the final value includes both a multiplication and a division by the mapped area. The multiplication and division cancel out and can both be excluded from the computation, leaving only the ray values and slab intersection lengths.

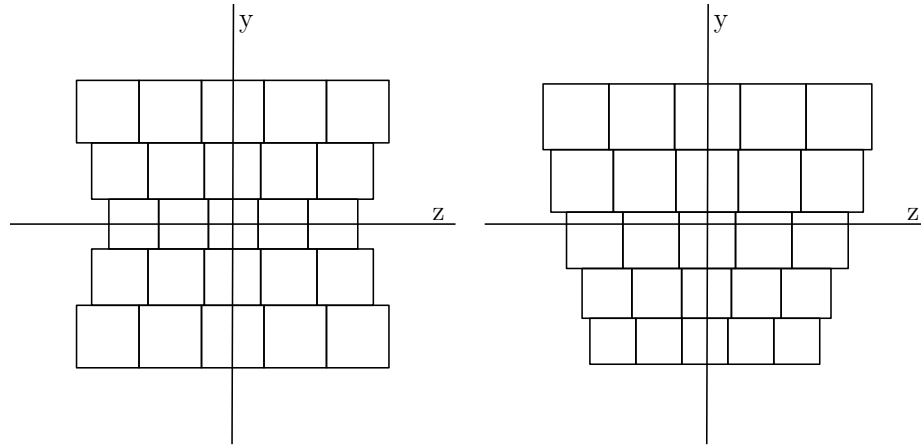


Figure 3.7: Detector array mapped to $y-z$ plane. Left: Mapped at an orthogonal angle (0°). Right: Mapped at a 45° angle.

Chapter 4

Implementation

4.1 Naive Branched Implementations

With the intent of implementing the distance-driven algorithm on a GPU, a CPU implementation was created, which computes ray and voxel values independently. During forward projection, this implementation loops over the rays. For each ray, it maps each voxel to the common plane and determines if there is overlap. This implementation greatly simplified the initial port of the reconstruction code from C++ to Cuda, but when run synchronously, it is exceptionally inefficient. It performs duplicate voxel mapping for every ray and does not take advantage of the uniformity of voxel mappings. The backprojection follows a similar process and has similar flaws.

In the explanation of the distance-driven system model in §3.2.1, it was mentioned that it is possible to implement the coordinate system and rotation such that the voxels rotate instead of the source and detector. Rotating the voxels removes the need to change which plane is being mapped to. For example, if the source is fixed to 0° , mapping will always be done to the y - z plane. It is necessary to determine which edges of the voxels to map, but this is only required when mapping voxels. In contrast, determining which plane is being mapped to is necessary throughout both the forward and backprojection kernels. Voxels are also simpler to rotate because they

always rotate about the origin, while detectors are rotated around the origin as the projection angle changes and rotated around the source position as the row changes. Despite these advantages, there is one significant downside to rotating voxels. Once voxels have been rotated with respect to the origin, image slabs are no longer parallel to the common plane and therefore do not map uniformly. As a result, it is preferable to rotate the source and detectors when using the distance-driven model.

This CPU implementation was ported to CUDA. The CUDA implementation consists of three different kernels. The forward projection kernel uses one thread per ray to compute the weighted projection data error $e = R(y - Ax)$, and the backprojection kernel uses one thread per voxel to compute the image update $u = CA^T e$. The final kernel uses a single thread per voxel to update the image approximation with the output of the backprojection kernel.

4.2 Branched Implementation

A synchronous branched implementation which better takes advantage of uniform mappings was also created. Since voxels in an image slab map uniformly to the common plane, the mapping of all voxels in an image slab can be simply computed using the mapping of just one voxel in that slab. Therefore, for each view it is only necessary to map the most negative voxel in each slab because the remaining voxel mappings can be computed by multiplying by the mapped width and the difference in index.

The mapping of the detectors is slightly more complicated. As described in §1.3, the rows of the detector panel are curved such that the center of each detector is normal with the source in the x - y plane. The detectors are completely flat along the columns. Therefore, rows of detectors are uniformly spaced, and we can determine the mappings for all detectors in a row for a specific view by mapping the first detector in that row.

Once the voxel and detector mappings have been determined, they are looped over to determine the overlaps. The forward and backprojection operations loop over each projection, processing all image slabs during each iteration. For each image slab, the computation is initialized with the most negative row of the image slab and detectors. The more negative of these rows is incremented until there is overlap. For each pair of overlapping rows the overlap is computed and weighted by the row height. This computation is shown in Figure 4.1.

```

if (voxel_row_boundary < detector_row_boundary)
{
    weighted_row_overlap =
        (voxel_row_boundary - previous_row_boundary) /
        detector_row_height;
    previous_row_boundary = voxel_row_boundary;
    voxel_row_boundary = next_voxel_row_boundary;
}
else
{
    weighted_row_overlap =
        (detector_row_boundary - previous_row_boundary) /
        detector_row_height;
    previous_row_boundary = detector_row_boundary;
    detector_row_boundary = next_detector_row_boundary;
}

```

Figure 4.1: Code excerpt from the branched distance-driven implementation showing the computation of weighted row overlap and incrementing of the current row

For each pair of overlapping rows, the computation is initialized with the most negative column from the image and detector row. The more negative of these columns is incremented until there is overlap. Then, for each pair of overlapping columns, the overlap is computed and weighted by the detector column width. The final weighted overlap which is a_{ij} for ray i and voxel j is computed by multiplying the slab intersection length and the weighted row and column overlaps. This value is added to the row sum for the current ray and multiplied by the current voxel value before being added to the current ray value. When the detector column is incremented, the current ray is updated and the new slab intersection length is computed. Figure 4.2 shows these calculations.

```

if (voxel_column_boundary < detector_column_boundary)
{
    weighted_column_overlap =
        (voxel_column_boundary - previous_column_boundary) /
        detector_column_width;
    weighted_overlap = slab_intersection_length *
        weighted_row_overlap * weighted_column_overlap;
    previous_column_boundary = voxel_column_boundary;
    voxel_column_boundary = next_voxel_column_boundary;
    current_voxel = next_voxel
}
else
{
    weighted_column_overlap =
        (detector_column_boundary - previous_column_boundary) /
        detector_column_width;
    weighted_overlap = slab_intersection_length *
        weighted_row_overlap * weighted_column_overlap;
    previous_column_boundary = detector_column_boundary;
    detector_column_boundary = next_detector_column_boundary;
    current_ray = next_ray;
    slab_intersection_length =
        getSlabIntersectionLength(current_ray);
}
row_sums[current_ray] += weighted_overlap;
ray_values[current_ray] += weighted_overlap *
    voxel_values[current_voxel];

```

Figure 4.2: Code excerpt from the branched distance-driven implementation showing the computation of column overlaps, elements of A , row sums, and ray values.

4.3 Branchless Implementations

In the inner loop of the branched distance-driven algorithm, the ray or voxel values are calculated by looping over the detector and voxel boundaries which have been mapped to a common plane. During each loop iteration, the computation will vary slightly depending on whether the next boundary is a detector or voxel boundary [22]. The behavior of this branch is hard to predict, which makes efficient execution on pipelined CPUs with branch prediction difficult. The branch is even more detrimental to performance when executed on a GPU because it causes frequent thread divergence. In 2006, De Man and Basu addressed this issue by developing a branchless variation of the distance-driven calculation, discussed in §3.2.3 [22]. The branchless distance driven algorithm was implemented both on a CPU and GPU. The GPU implementation is described here. The CPU implementation is similar but lacks the features specific to the GPU.

During forward projection, each thread computes the value for a single ray. The thread maps the detector to the common plane and then iterates through each plane of the integral image. The mapped detector edges are constrained to the integral image plane and the integral image is accessed at the four corners of the mapped detector to compute (3.3). For backprojection, each thread computes the value for a single voxel. Because the mapped detectors are not uniform, the integral rays must be recomputed and the backprojection operation must be performed separately for each projection.

4.3.1 Computation of Integral Image and Integral Rays

Given their role as graphics processing hardware, GPUs contain a specialized cache for texture memory and are capable of performing bilinear interpolation to access values from 2D texture data. Cuda allows the programmer to store arbitrary floating-point data in texture memory and allows read access inside kernels run on the GPU. There are two advantages to storing the integral image and integral rays in texture memory. The first is that the texture cache provides 2D spatial locality. This is ideal, because the memory access pattern into these integral data structures will often require values from indices spanning multiple nearby rows and columns. The second is the built-in interpolation is faster in execution and simpler to implement than manual interpolation, though at reduced precision. It is possible to store the integral image and rays in texture memory while still using manual interpolation; however, the difference in reconstruction time is significant. The iteration time for a 256x256x256 image with 720x56 detectors and 5000 projections increased by 22.2% when using manual interpolation instead of the built-in texture interpolation.

As described in §3.2.3, when creating the integral image, each voxel value is multiplied by its mapped area before being summed. However, because voxel mappings along an image slab are uniform, the mapped area will be a constant value for each integral image. This allows the area to be factored out of the summations

and applied directly to each computed ray value. Once the mapped area is factored out of the computation of the integral image, the integral image becomes independent of the current projection and needs only be computed once per iteration per common plane. The creation of the integral image is performed by three different Cuda kernels. The first sums voxel values along image slab rows (in the z direction) with one thread per row and saves the result into a vector for the y - z common plane. This step is the same for both the x - z and y - z common plane, so the results of this kernel can be copied and reordered to obtain the equivalent vector for the x - z common plane. The next two kernels each take either the y - z or x - z integral image and sum along image slab columns with one thread per column.

Each column in the integral image is logically separated from the next by the width of a mapped voxel and each row is logically separated by the height of a mapped voxel. Therefore, to access integral image values, coordinate locations must be transformed into integral image locations. This is done in the z dimension by subtracting the coordinate location by the coordinate location of the first voxel in the slab and dividing by the width of the mapped voxel. The process is similar for the x/y dimension, but division is by the mapped voxel height.

The mapped detectors are not uniform, therefore, additional steps must be taken when computing the integral rays. The original description of the branchless distance-driven model omits a full explanation about how this non-uniformity is managed and alludes to an upcoming paper, which does not seem to be available [22]. The partial explanation provided makes use of the fact that the calculation of overlap area is constant for any voxel and ray pair and is independent of the forward or backprojection steps. It is suggested to apply flow-graph reversal techniques to the projection kernel and interpolate from voxel values to ray values. In this case, interpolation is defined as the “adjoint or transpose operation to interpolation” [22]. A 2016 paper authored by Liu et al. discusses a Cuda implementation of the branchless distance-driven algorithm. In the backprojection step, it does not mention flow graph reversal techniques or interpolation, but states that integral volumes are

generated for every projection view. This implies the integral rays are computed in the same way as the integral image; however, it does not discuss the non-uniformity of detector mappings [11].

In order to create the integral rays, a fixed width and height are chosen for the integral ray elements. The integral ray data structure will contain a sufficient number of rows and columns to completely enclose the area of the mapped detectors. Interpolation is then used to resample the ray values multiplied by their slab intersection lengths into this new grid. The interpolated values are then summed along rows and columns in the same way as the integral image. In practice, one kernel sums and interpolates ray values multiplied by their slab intersection lengths along rows with one thread per detector row. A second kernel sums and interpolates along columns of the integral rays with one thread per column of the integral ray data structure. Figure 4.3 illustrates the integral ray data structure in relation to the mapped detectors.

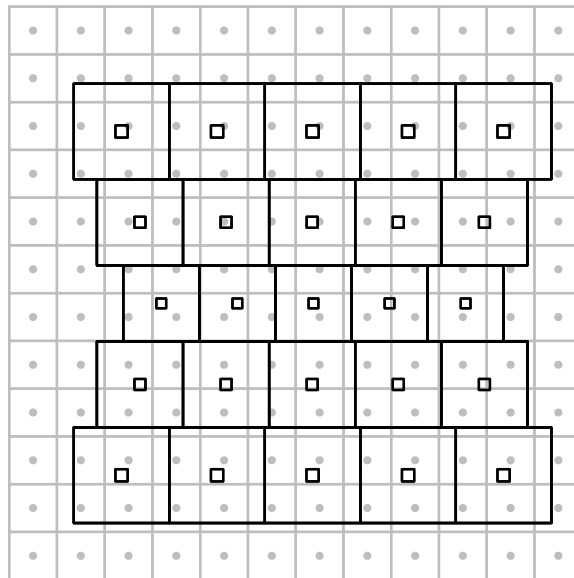


Figure 4.3: Interpolation from detector elements mapped at an orthogonal angle to a uniform grid. The value of the grey circles are determined from the nearby squares.

The fixed width and height of the integral ray elements allows coordinate locations to be transformed into integral ray locations by subtracting the location of the first

integral ray element from the coordinate location and dividing by the respective width or height.

Chapter 5

Results and Discussion

5.1 Performance Comparison

Figure 5.1 compares the execution time of a single iteration of the various implementations of distance-driven based reconstruction. Results were collected on a system with an Intel Core i5-6600 CPU that runs at 3.3 GHz. Note that CPU performance was evaluated using a single core. The system's GPU is an NVIDIA GTX 970 which has 4 GB of onboard memory and 1664 cores that run at 1279 MHz. The CPU naive branched implementation performs a significant amount of duplicate computation as described in §4.1 and as expected performs poorly. It does not take advantage of uniform mappings, computes all voxel mappings for each ray during forward projection, and computes all ray mappings for each voxel during backprojection. The GPU naive branched implementation described in §4.1 performs the same computations with the advantage of the parallelism provided by the GPU but suffers from frequent branch divergence and offers only a slight performance improvement. The branchless CPU implementation removes the branch inside of the inner loop, takes advantage of mapped voxel uniformity and the uniformity of mapped detector rows. As a result, it executes faster than the naive implementations. The branchless GPU implementation further improves on the CPU implementation

by parallelizing execution. It also benefits from the texture memory 2D cache and fast interpolation. As a result, it executes significantly faster than the other implementations. The branched implementation described in §4.2 performs negligibly slower than the branchless CPU implementation but performance results have been omitted. Although not implemented, a branched GPU implementation would be expected to have better performance than the naive and CPU implementations but still be slower than the branchless GPU implementation due to thread divergence and the inability to take advantage of texture memory. Figure 5.2 shows the speedup provided by the GPU branchless implementation when compared to the CPU branchless implementation.

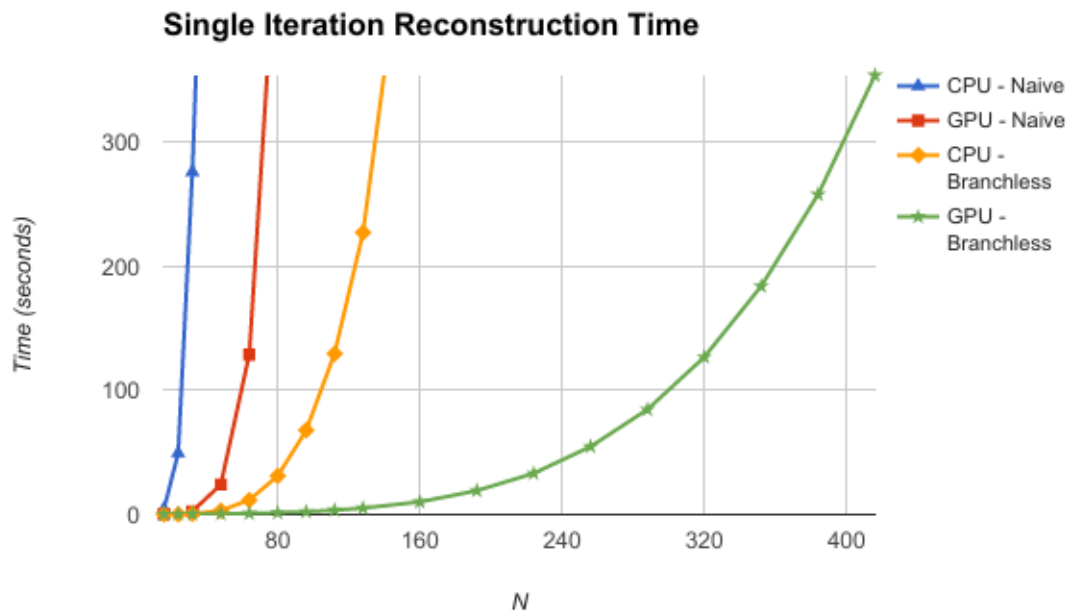


Figure 5.1: The single iteration reconstruction time in seconds of the various implementations as the problem size increases. N is the number of image and detector rows and columns, the image depth, and the number of projections. Therefore, this is a system of N^3 equations and N^3 variables.

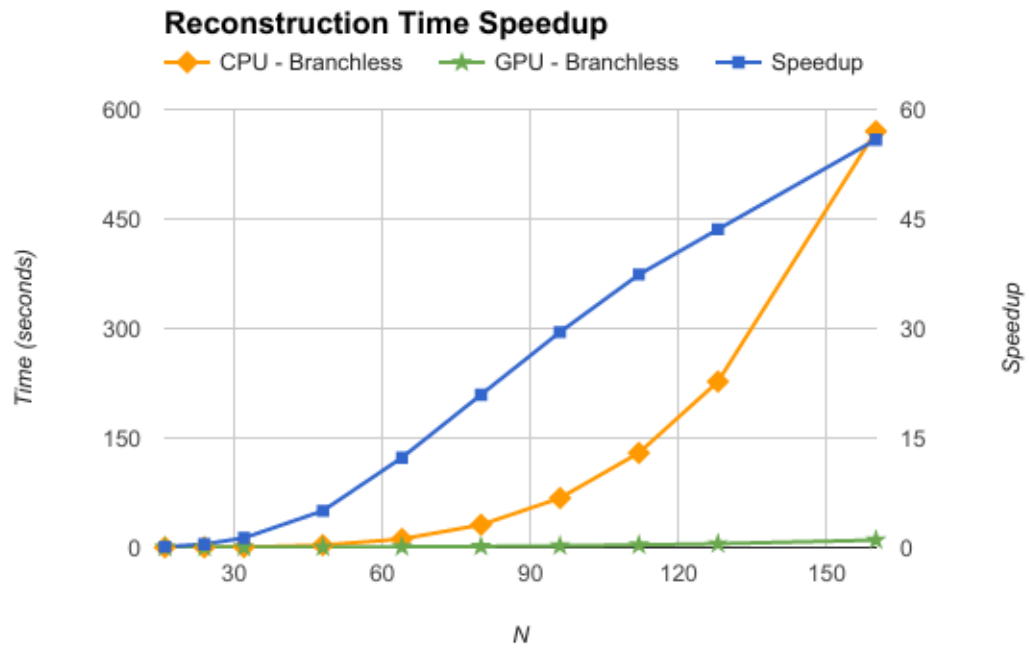


Figure 5.2: The speedup of the single iteration reconstruction time between the GPU and CPU branchless distance-driven implementations. N is the number of image and detector rows and columns, the image depth, and the number of projections. Therefore, this is a system of N^3 equations and N^3 variables.

5.2 Potential Performance Improvements

None of the implementations presented in this paper have been thoroughly optimized. There is potential to make both algorithmic and implementation improvements in order to increase the performance. The focus of this section will be on the branchless implementation.

Every section of the code which creates or uses detector/voxel mappings must check for the current view angle and adjust its behavior depending on which common plane is to be used. This is not an issue for the backprojection kernel or the integral ray creation kernels because they are executed separately for each view. However, this could lead to thread divergence in the forward projection kernel. Divergence will occur when rays from two different views, which map to different planes, are processed by threads in the same warp of 32 threads. This is an infrequent occurrence because projections are assigned to threads in-order and therefore there are only four such pairs of views per full rotation. Despite this infrequency, it would be advantageous to restrict the assignments of rays to threads such that all threads in a warp map to the same plane.

Increasing the number of elements computed per thread could lead to an overall decrease in reconstruction time. For example, in order for a thread in the backprojection kernel to calculate an image value it must access four points from the integral rays. Because the voxel mappings within an image slab are uniform, two of these points are shared with each adjacent voxel. Therefore, if each thread calculated the value for two voxels instead of one, the number of integral ray accesses would decrease by 25%.

5.3 Image Quality

5.3.1 Floating-Point Precision

GPUs are known for their high performance single-precision floating-point computations but often take much longer to execute when using double-precision floating-point values. The GPU used for experimentation is an NVIDIA GTX 970, which has a Maxwell architecture. The Maxwell architecture typically executes double-precision operations 32 times slower than single-precision operations [23]. As a result, it is highly desirable to minimize the number of double-precision values used. Fortunately, the projection data and image output are single-precision. Because the projection data is noisy and the reconstruction process is simply an approximation, single-precision values are sufficient to produce good quality reconstructions.

5.3.2 Texture Interpolation

Cuda texture interpolation is performed using only 8 bits to represent the fractional part of the texture fetch location. Therefore, there is potential for precision errors to be introduced into the calculations of ray and voxel values. In general, this low precision interpolation does not noticeably affect any output. However, there is at least one case where it does. If image voxels are much larger in size than detectors, visible noise will be introduced. The low precision interpolation can be thought of as a piecewise or stair-stepping function. The primary cause of the noise is that the coordinates of the mapped detector corners are close enough together in relation to the mapped voxels that multiple corners will interpolate to the same step and produce equivalent values, while other corners may interpolate to either side of a step and their difference will be exaggerated. This noise can be demonstrated by examining the row sum values for a view. This is illustrated in Figure 5.3, where texture interpolation with a voxel size to detector size ratio of 5.18 to 1 shows visible noise in the selected

view, a ratio of 2.59 to 1 shows slight noise, and a ratio of 1.29 to 1 shows almost no noise. In all cases, the manual interpolation shows no noise.

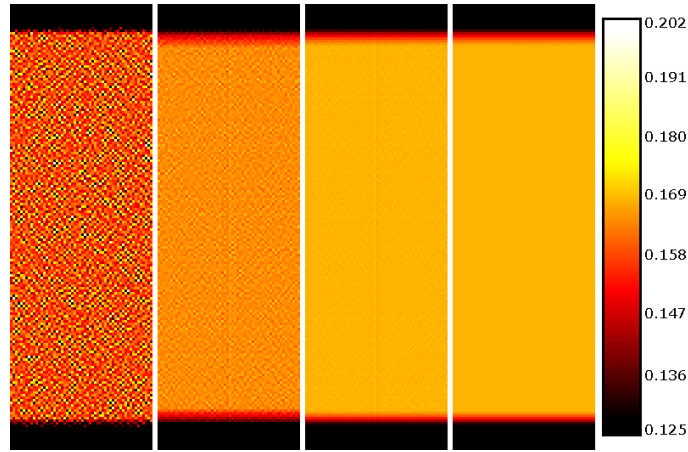


Figure 5.3: Comparison of row sum values produced with various voxel size to detector size ratios. In order: texture interpolation with 5.2:1 ratio, texture interpolation with 2.6:1 ratio, texture interpolation with a 1.3:1 ratio, and manual interpolation which is uniform for all ratios.

5.3.3 Border Elements

It is possible for X-rays to be attenuated by material outside the area covered by the image voxels. If those rays do not overlap with any voxels, they will be ignored. If they do overlap with voxels, those voxels will have the out-of-image attenuation attributed to them. This may harm image quality especially if a ray intersects only partially with a single voxel. This results in an extremely small row sum value and the entirety of the ray's attenuation will be attributed to a fraction of a single voxel. Consider the first iteration where the value of the voxel will be zero. Let the system matrix value for this ray and voxel be ϵ and note it is equal to the row sum because the ray overlaps with this voxel only. Therefore, the output of forward projection for this ray will be $(y_i - 0 * \epsilon) / \epsilon$ and because ϵ is so small, the ray's value may be orders of magnitude larger than the other rays. In theory, this is not an issue because during backprojection, this value will be again multiplied by the system matrix value, ϵ . However, the interpolation performed during the creation of the integral detectors

allows this ray to potentially affect voxels it does not intersect. This is discussed in §5.3.4. The first potential solution was to simply ignore rays with very small row sums. The difficulty in implementing this solution is deciding which value should be the smallest allowable row sum as the range of appropriate values is dependent on the system geometry and number of voxels. It is also not ideal to remove or ignore any information which could be used to reconstruct the image. Experimentation showed that with a simple bound, it was not possible to avoid these “bad” rays without also removing “good” rays.

The working solution is to create a logical border of extra voxels around the image when calculating the row sums. These border voxels will overlap with rays that only barely overlap the real voxels. This will result in more realistic row sum values for these rays and will both prevent extremely small row sums, as well as reduce the effect of out-of-image attenuation. The number of border voxels necessary is related to the ratio between voxel and detector sizes. If detectors are larger than voxels, more voxels will be required to sufficiently balance row sum values. Figure 5.4 shows a comparison of forward projection output from the image quality bag. The output without border voxels has a clear border around the image and has highly valued rays along the edge of the image. The output with the border voxels lacks all such issues.

Note border voxels are only needed when using SIRT to solve an R weighted least squares problem, as the row sum values have the potential to be very small. When solving the statistically weighted least squares problem described in §2.2, division by single row sums is not performed. Therefore, border elements are not a necessity.

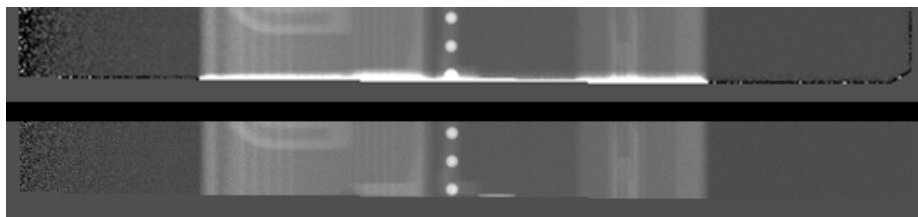


Figure 5.4: Comparison of forward projection output of an 128x128x10 image with three border voxels (below) and with no border voxels (above). Images are cropped from a single view of the image quality bag and rotated 90°.

5.3.4 Ray Value Leakage

A drawback of the interpolation used when summing along rows to create the integral rays happens when accessing values through interpolation; there is a chance the resulting value will be influenced by rays it would not have been influenced by otherwise. For example, with linear interpolation, a queried value could be influenced by three rays instead of two. The cause of this is illustrated in Figure 5.5. The top level of values have been resampled to a finer granularity in the second level. When querying point P from the top level, its value would be a function of point A and B . However, if point P is queried using the second level, its value will be a function of ab and bc and since bc is computed from B and C , the value of P will be influenced by points A , B , and C . As a result, rays which come very close to but do not intersect a voxel have a chance to affect or leak into that voxel's value. This is not ideal, but does not appear to significantly affect image quality. Note that for this to happen, the incorrect ray value will have a small weight. For example, in Figure 5.5, C makes a small contribution to bc and bc makes a small contribution to P . Despite this, ray leakage can become an issue if there are adjacent rays with extreme differences in value. This generally does not happen unless there is something wrong with the data or calculations. For example, the extremely large ray values created when there are no border voxels used during forward projection can leak into voxels they do not intersect. The results of this leakage in forward projection output are illustrated in Figure 5.6. The top image is the same as in Figure 5.4 and shows the high valued rays which partially intersected the edge of the image and had very small row sums. The bottom image shows the same rays after a second iteration. Some of the rays still have large positive values while other rays have large negative values. The negative valued rays are rays which overlap with voxels whose values have been artificially inflated by the ray value leakage in the backprojection. The effect of a lack of border voxels and ray value leakage on the reconstructed image is illustrated in Figure 5.7 which shows a slice through one of the small metal spheres of the image quality bag.

The slice shown is the last slice of the reconstructed image, and therefore there are many rays which have only partial intersections with these voxels.

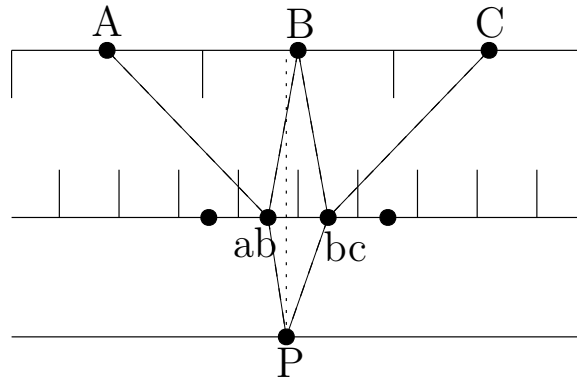


Figure 5.5: Illustration of ray value leakage in the integral rays

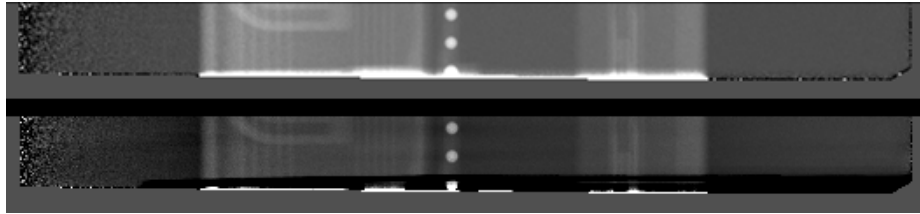


Figure 5.6: The effects of ray value leakage. Top: first iteration with no border voxels. Bottom: second iteration with no border voxels. Images are cropped from a single view of the image quality bag and rotated 90°. White elements have large positive values and black elements have large negative values.

5.3.5 Reconstructed Images

Figures 5.8 and 5.9 show the results of reconstruction over 57 and 54 iterations for the image quality and resolution bags, respectively. In each figure, the top image shows a slice through the y - z plane, the middle image shows a slice through the x - z plane, and the bottom image shows a slice through the x - y plane. In the image quality bag reconstruction, the aluminum bar and metal beads are the most attenuating objects in the bag, and they produce very slight metal artifacts. The delrin block is less attenuating than the metal objects but creates more artifacts due to scatter as can be seen in the top image. The objects in the resolution bag reconstruction are

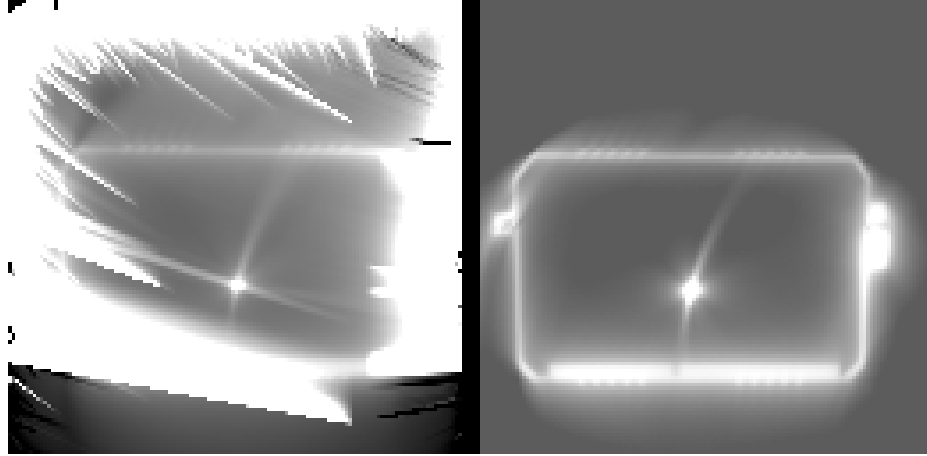


Figure 5.7: Slice through a small metal sphere of the image quality bag. The last slice of the reconstructed image. Left: image with artifacts created by a lack of border voxels and ray value leakage. Right: image produced when using border voxels.

significantly less clear than those in the image quality bag. This is a result of the large and highly attenuating lead block. In the top and bottom images, significant artifacts are visible. In the middle image, the less attenuating (blue) features of the bag are not visible in the area parallel to the lead block. This is likely because the lead block has attenuated a majority of the X-rays travelling through that area.

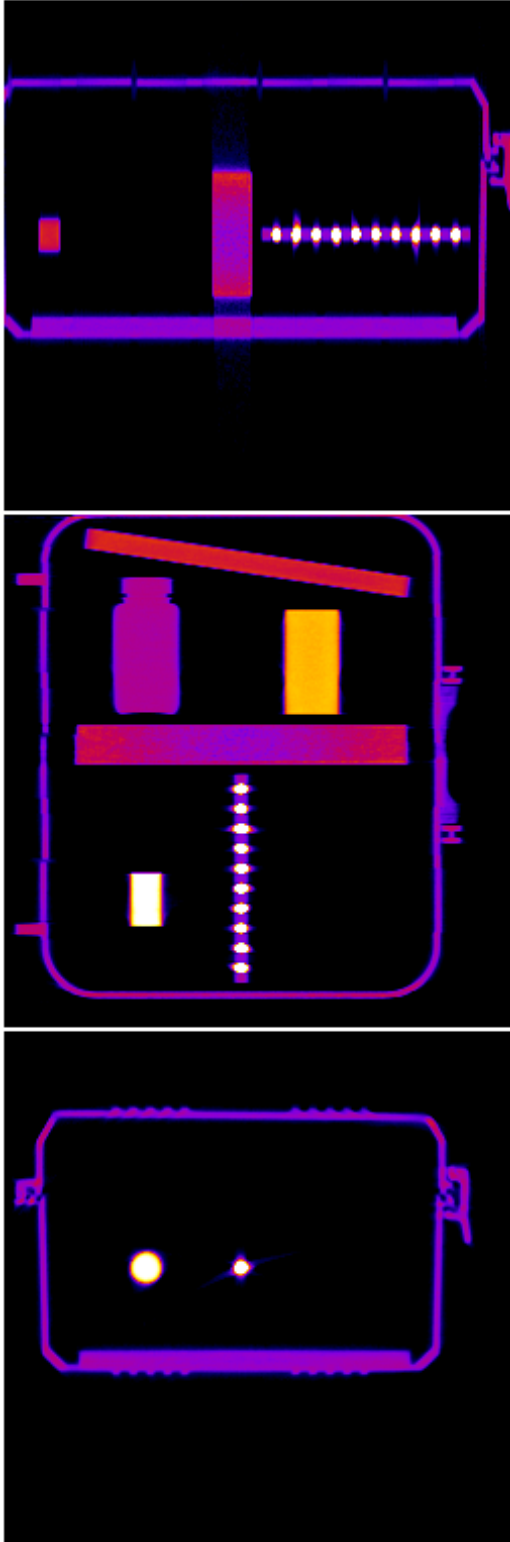


Figure 5.8: Reconstruction of image quality bag

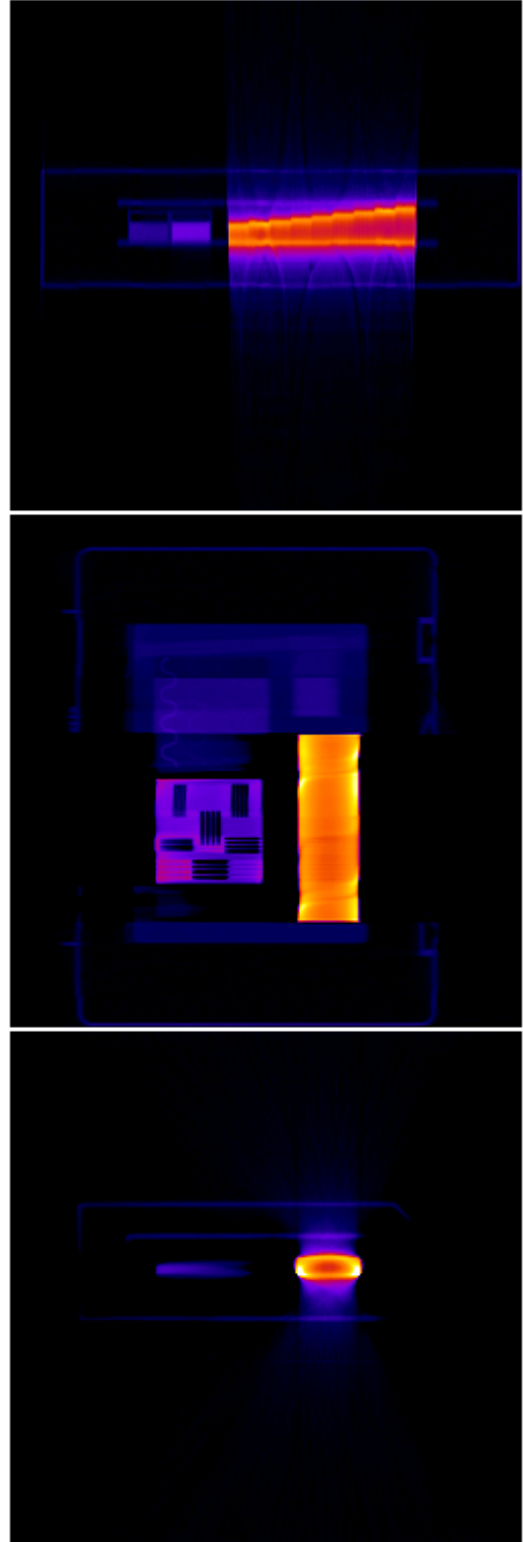


Figure 5.9: Reconstruction of resolution bag

Chapter 6

Conclusion

The efficiency of the distance-driven system model's computation can be improved upon by using the branchless distance-driven variation. Unfortunately, this variation leads to additional issues which must be overcome, especially for the backprojection operation. During forward projection, the uniformity of voxel mappings makes the generation of the integral image straightforward and allows for the removal of the conditional in the inner loop of the distance-driven computation. This advantage is also relevant to the backprojection, but the lack of uniformity in the detector mappings complicates the generation of the integral rays. The solution presented is to create a grid large enough to contain the current projection and interpolate the ray values onto the grid. Values are then summed along rows and columns to produce the integral rays. Interpolation to a finer grid allows for some slight leakage of ray values into voxels they map adjacent to but do not intersect; however, this does not appear to visibly affect the image quality as long as there are no erroneously large ray values. Such erroneous values can be created by very small system matrix row or column sums when calculating ray or voxel values. Small row and column sums are a result of defining a discrete image which may only partially intersect with some rays. The solution presented is to surround the image and detectors with additional elements when computing the row and column sums, ensuring they have reasonable

values. Texture memory available on GPUs has been shown to provide significant advantages for accessing the integral image and integral rays. The 2D spatial locality provided is a good fit for the access pattern, and the ability to perform low precision built-in interpolation during access greatly decreases the overall reconstruction time in comparison to manual software interpolation. The branchless implementation is able to reconstruct an image significantly faster than the other implementations presented here; however, room for improvement remains. Potential areas of improvement include more carefully organizing threads in the forward projection kernel to avoid branch divergence, and increasing the number of elements computed per thread in both the forward projection and backprojection kernels.

Bibliography

- [1] Sameer Singh and Maneesha Singh. “Explosives Detection Systems (EDS) for Aviation Security”. In: *Signal Processing* 83.1 (2003), pp. 31–55.
- [2] Matthew Merzbacher and Todd Gable. “Applying Data Mining to False Alarm Reduction in an Aviation Explosives Detection System”. In: *Security Technology (ICCST), 2010 IEEE International Carnahan Conference on*. IEEE. 2010, pp. 161–164.
- [3] Thomas M Benson. “Iterative Reconstruction of Cone-Beam Micro-CT Data”. PhD thesis. University of Tennessee, Knoxville, 2006.
- [4] Avinash C Kak and Malcolm Slaney. *Principles of Computerized Tomographic Imaging*. SIAM, 2001. Chap. 3, 7.
- [5] Jiang Hsieh et al. “Recent Advances in CT Image Reconstruction”. In: *Current Radiology Reports* 1.1 (2013), pp. 39–51.
- [6] Jens Gregor and Jeffrey A Fessler. “Comparison of SIRT and SQS for Regularized Weighted Least Squares Image Reconstruction”. In: *IEEE Transactions on Computational Imaging* 1.1 (2015), pp. 44–55.
- [7] Anders H Andersen. “Algebraic Reconstruction in CT from Limited Views”. In: *IEEE Transactions on Medical Imaging* 8.1 (1989), pp. 50–55.
- [8] Bernard E Oppenheim. *Reconstruction Tomography from Incomplete Projections*. Tech. rep. Chicago Univ., Ill.(USA). Dept. of Radiology; Franklin McLean Memorial Research Inst., Chicago, Ill.(USA), 1975.
- [9] Jean-Baptiste Thibault et al. “A Three-Dimensional Statistical Approach to Improved Image Quality for Multislice Helical CT”. In: *Medical Physics* 34.11 (2007), pp. 4526–4544.
- [10] Daniel Schlifske and Henry Medeiros. “A Fast GPU-Based Approach to Branchless Distance-Driven Projection and Back-Projection in Cone Beam CT”. In: *SPIE Medical Imaging*. International Society for Optics and Photonics. 2016, 97832W–97832W.

- [11] Rui Liu et al. “GPU Acceleration of Branchless Distance Driven Projection and Backprojection”. In: *4th International Conference on Image Formation in X-Ray Computed Tomography, Bamberg, Germany*. 2016.
- [12] CUDA Nvidia. “Nvidia Cuda C Programming Guide”. In: *Nvidia Corporation* 120.18 (2011).
- [13] Jens Gregor and Thomas Benson. “Computational Analysis and Improvement of SIRT”. In: *IEEE Transactions on Medical Imaging* 27.7 (2008), pp. 918–924.
- [14] Ken Sauer and Charles Bouman. “A Local Update Strategy for Iterative Reconstruction from Projections”. In: *IEEE Transactions on Signal Processing* 41.2 (1993), pp. 534–548.
- [15] H Malcolm Hudson and Richard S Larkin. “Accelerated Image Reconstruction Using Ordered Subsets of Projection Data”. In: *IEEE Transactions on Medical Imaging* 13.4 (1994), pp. 601–609.
- [16] Robert L Siddon. “Fast Calculation of the Exact Radiological Path for a Three-Dimensional CT Array”. In: *Medical Physics* 12.2 (1985), pp. 252–255.
- [17] Filip Jacobs et al. “A Fast Algorithm to Calculate the Exact Radiological Path Through a Pixel or Voxel Space”. In: *CIT. Journal of Computing and Information Technology* 6.1 (1998), pp. 89–94.
- [18] Gengsheng L Zeng and Grant T Gullberg. “A Study of Reconstruction Artifacts in Cone Beam Tomography Using Filtered Backprojection and Iterative EM Algorithms”. In: *IEEE Transactions on Nuclear Science* 37.2 (1990), pp. 759–767.
- [19] Lizhe Xie et al. “An Effective CUDA Parallelization of Projection in Iterative Tomography Reconstruction”. In: *PLOS ONE* 10.11 (2015), e0142184.
- [20] Bruno De Man and Samit Basu. “Distance-Driven Projection and Backprojection”. In: *Nuclear Science Symposium Conference Record, 2002 IEEE*. Vol. 3. IEEE. 2002, pp. 1477–1480.

- [21] Bruno De Man and Samit Basu. “Distance-Driven Projection and Backprojection in Three Dimensions”. In: *Physics in Medicine and Biology* 49.11 (2004), p. 2463.
- [22] Samit Basu and Bruno De Man. “Branchless Distance Driven Projection and Backprojection”. In: *Electronic Imaging 2006*. International Society for Optics and Photonics. 2006, 60650Y–60650Y.
- [23] Lukas Polok and Pavel Smrz. “Increasing Double Precision Throughput on NVIDIA Maxwell GPUs”. In: *Proceedings of the 24th High Performance Computing Symposium*. Society for Computer Simulation International. 2016, p. 20.

Vita

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